## 博士学位論文

咽頭癌に対する知識ベース放射線治療計画の線量体 積ヒストグラム解析

近畿大学大学院医学研究科医学系専攻

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### **Doctoral Dissertation**

Dose-volume histogram analysis and clinical evaluation of knowledge-based plans with manual objective constraints for pharyngeal cancer

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#### 論文題目

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# Dose-volume histogram analysis and clinical evaluation of knowledge-based plans with manual objective constraints for pharyngeal cancer

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#### ABSTRACT

The present study aimed to evaluate whether knowledge-based plans (KBP) from a single optimization could be used clinically, and to compare dose–volume histogram (DVH) parameters and plan quality between KBP with (KBP<sub>CONST</sub>) and without (KBP<sub>ORIG</sub>) manual objective constraints and clinical manual optimized (CMO) plans for pharyngeal cancer. KBPs were produced from a system trained on clinical plans from 55 patients with pharyngeal cancer who had undergone intensity-modulated radiation therapy or volumetric-modulated arc therapy (VMAT). For another 15 patients, DVH parameters of KBP<sub>CONST</sub> and KBP<sub>ORIG</sub> from a single optimization were compared with CMO plans with respect to the planning target volume (D<sub>98%</sub>, D<sub>50%</sub>, D<sub>2%</sub>), brainstem maximum dose (D<sub>max</sub>), spinal cord D<sub>max</sub>, parotid gland median and mean dose (D<sub>med</sub> and D<sub>mean</sub>), monitor units and modulation complexity score for VMAT. The D<sub>max</sub> of spinal cord and brainstem and the D<sub>med</sub> and D<sub>mean</sub> of ipsilateral parotid glands were unacceptably high for KBP<sub>ORIG</sub>, although the KBP<sub>CONST</sub> DVH parameters met our goal for most patients. KBP<sub>CONST</sub> and CMO plans produced comparable DVH parameters. The monitor units of KBP<sub>CONST</sub> were significantly lower than those of the CMO plans (P < 0.001). Dose distribution of the KBP<sub>CONST</sub> was better than or comparable to that of the CMO plans for 13 (87%) of the 15 patients. In conclusion, KBP<sub>ORIG</sub> was found to be clinically unacceptable, while KBP<sub>CONST</sub> from a single optimization was comparable or superior to CMO plans for most patients with head and neck cancer.

Keywords: intensity-modulated radiation therapy; knowledge-based planning; nasopharyngeal cancer; oropharyngeal cancer; volumetric-modulated arc therapy

#### INTRODUCTION

The clinical use of intensity-modulated radiation therapy (IMRT) and volumetric-modulated arc therapy (VMAT) represents significant advances in radiation therapy. IMRT is effective, especially in patients with head and neck cancer, because the clinical target volumes (CTV) generally border organs at risk (OARs) such as the salivary glands, brainstem and spinal cord [1]. However, several clinical limitations are associated with the planning of IMRT for head and neck cancer. These include (i) the time-consuming optimization process, (ii) the achievable dose-volume histogram (DVH) being unknown at the time of optimization, and (iii) the dependence of plan quality on the planners' (or institutions') experience and skills [2–11].

One approach that can be used to improve speed and efficiency and reduce variability in treatment planning is the so-called knowledge-based plans (KBP) approach. KBP are defined as any approach that directly uses prior experience to either predict an achievable dose for a new patient or to derive a better starting point for optimization by a planner [12]. Rapidplan<sup>TM</sup>, a commercial KBP tool, is integrated into the Eclipse (Varian Medical Systems, Palo Alto, USA) treatment planning system (TPS) and is a machine-learning tool that uses best practices from previous treatment plans to create knowledge-based models for the treatment of new patients. Comparisons of KBP with clinical manual optimized (CMO) plans for prostate cancer have demonstrated that KBP can lead to clinically acceptable DVHs [2, 5, 6, 12–14].

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Fewer reports have compared KBP with CMO plans in head and neck cancer than in prostate cancer [12], although most investigators have demonstrated that KBP are advantageous for DVH analysis of head and neck cancer [3, 4, 7, 8, 15]. We consider it is clinically important to accurately establish the usefulness of KBP based on various reports. Several investigators did not set objective constraints manually for OARs [3, 4, 7, 16]. Wang et al. did not separate the training and validation sets [8], while Krayenbuehl et al. did not evaluate the DVH of brainstem [15]. In addition, Chang et al. reported that reoptimization of KBP was required for nasopharyngeal cancer (NPC), because the KBP DVH parameters for neurological structures were poorer than those of CMO plans [11]. We therefore sought to establish the advantage of KBP for head and neck cancer with or without objective constraints for OARs.

The present study aimed to evaluate whether KBP from a single optimization could be used in clinical settings by adding objective constraints manually. Thus, in the present study, KBP without manual setting of objective constraints (KBP<sub>ORIG</sub>) and those with objective constraints (KBP<sub>CONST</sub>) were compared with CMO plans for patients with NPC or oropharyngeal cancer (OPC).

#### MATERIALS AND METHODS Patient selection and contouring

A training set of 55 clinical plans for NPC or OPC treated by IMRT or VMAT between 2014 and 2018 was used to train the KBP. Treatment plans were VMAT in 12 cases (22%) and IMRT in 43 cases (78%). As our institution adopted the VMAT technique from 2016, the number of VMAT plans was small in the training set. Staging was performed according to the tumor-node-metastasis (TNM) classification system (7th edition) of the International Union Against Cancer (UICC). As a validation set, further 15 clinical VMAT plans between 2017 and 2018 were used to compare the single-optimization KBP with CMO plans. Since the patients were recruited in a consecutive manner, the number of NPC patients was low in the validation set. As all patients were treated with whole neck irradiation, treatment plans were similar for NPC and OPC. All CMO plans were used clinically for the 15 patients. The characteristics of patients whose plans were used for training and validation are summarized in Table 1.

All patients were immobilized and thermoplastic masks were used to cover the head, neck and shoulders (Type-S thermoplastic-based system; MED-TEC, Orange City, IA, USA). Contrast-enhanced computed tomography (CT) scans for treatment planning were obtained at 2-mm slice intervals from the head to the aortic arch [17, 18]. CTV encompassed a 5.0-10.0 mm margin with appropriate anatomical correction around the gross tumor volume. The prophylactic nodal CTV was defined and delineated according to the Danish Head and Neck Cancer Group, the European Organization for Research and Treatment of Cancer, the French Group of Radiation Oncology for Head and Neck Cancer, the French Head and Neck Cancer Group, the National Cancer Institute of Canada and the Radiation Therapy Oncology Group consensus guidelines [19]. The nasopharyngeal or oropharyngeal region, the bilateral level II-IV nodes and the retropharyngeal nodes were included in the initial CTV [20]. Submandibular lymph nodes (level Ib) were only included in the CTV where their involvement was suspected. Margins of 3.0-4.0 mm were added to the

Table 1. Characteristics of patients in the training and validation sets

	Training set $(n = 55)$	Validation set $(n = 15)$
Age, years (median; range)	68; 28–89	61; 40–78
Male/female	36 (66%)/19 (34%)	14 (93%)/1 (7%)
Primary sites		
Nasopharyngeal cancer	19 (35%)	1 (7%)
Oropharyngeal cancer	36 (65%)	14 (93%)
TNM stage (7th edition)		
I	7 (13%)	0 (0%)
П	8 (15%)	0 (0%)
III	11 (20%)	3 (20%)
IVA	20 (36%)	8 (53%)
IVB	7 (13%)	4 (27%)
IVC	2 (3%)	0 (0%)

CTVs to determine the planning target volume (PTV), thus allowing for errors associated with treatment set-up and internal organ motion error [21]. The brain, brainstem, inner ears, eyes, larynx, lens, pharyngeal constrictor muscles, optic nerves, chiasm, mandible bone, oral cavity, spinal cord, parotid glands and thyroids were included as OARs at our institution. A 3.0-mm margin was added to the spinal cord as planning organ at risk volume (PRV). No margin was added to the parotid glands, and parotid glands minus PTV were used for treatment planning whereas DVH parameters were evaluated for each parotid gland. The treatment planning CTs and delineated structures used for the CMO plans were also applied to KBP, using the same methods.

#### Dose prescription and treatment planning

A two-step IMRT method is used at our institution instead of the simultaneous integrated boost method [1, 17, 18]. In the initial planning, the prescribed dose was 70 Gy in 35 fractions to the initial PTV. After whole-neck radiotherapy of 44–50 Gy in 22–25 fractions had been delivered in the initial plans, a boost plan was administered to the high-risk CTV up to a total dose of 70 Gy in 35 fractions. In the present study, the KBP and CMO plans were compared with the initial plans for the whole-neck region. The prescribed dose was normalized to the dose of 70 Gy to 95% of the PTV [18]. Our goals and acceptable criteria for DVH parameters are shown in Table 2.

All IMRT plans in the training set were created using Eclipse ver. 7.3.10 (Varian Medical Systems, Palo Alto, USA) and optimized with a dose volume optimizer. These IMRT plans were delivered using a dynamic multileaf collimation from one of two linear accelerators (Clinac 600C or Clinac 21EX; Varian Medical Systems, Palo Alto, USA) equipped with a 40-leaf dynamic multileaf collimator. Beam energies of 4 or 6 MV X-rays were used.

All VMAT plans for the training and validation sets were created using an Eclipse TPS ver. 13.6 with 6 or 10 MV photon beams. Two

Table 2. Our DVH goal and acceptable criteria for PTV and OARs

	Parameter	DVH goal	Acceptable criteria
PTV*	$D_{98\%}$	>93%	>90%
	$D_{50\%}$	<105%	<107%
	$D_{2\%}$	<120%	<125%
Spinal cord	$\mathbf{D}_{\mathrm{max}}$	<50.0 Gy	<54.0 Gy
Brainstem	$\mathbf{D}_{\max}$	<54.0 Gy	<64.0 Gy
Parotid gland <sup>b</sup>	$\mathbf{D}_{\mathrm{med}}$	<20.0 Gy	<24.0 Gy
8.73	$\mathbf{D}_{\mathrm{mean}}$	<26.0 Gy	<30.0 Gy

<sup>\*100%</sup> doses were set to 70 Gy

full arcs of VMAT were applied (gantry angle: 181-179° clockwise and 179–181° counterclockwise; collimator angles: 5 and 85°, or 30  $\,$ and 330°). The control point spacing was 2° of angular separation. All VMAT plans were optimized with a photon optimizer and calculated using the Varian analytic anisotropic algorithm and an Eclipse TPS for a TrueBeam (Varian Medical Systems, Palo Alto, USA) with a Millennium 120 multileaf collimator.

#### Model configuration for the knowledge-based optimized plans

The KBP model configuration and training process is described in previous reports [2, 14, 22]. In the KBP optimization process, optimization objectives named 'line objectives' were upper objectives placed on line and along the inferior DVH prediction boundary for OARs, and priority values were automatically generated (KBP<sub>ORIG</sub>). In addition, we could modify objective constraints for OARs manually after generating objective constraints automatically (KBPCONST). For both KBP<sub>ORIG</sub> and KBP<sub>CONST</sub>, objective constraints for the PTV needed to be manually set. In this study, the upper and lower objectives for the PTV were set at 70-70.7 Gy and 67.9-69.3 Gy, respectively for both KBPORIG and KBPCONST. Most previous investigators used only automatically generated objective constraints for OARs and compared the DVH parameters between the KBP and CMO plans [2, 4, 6, 7, 11, 13-15, 22, 23]. Alternatively, Kamima et al. reported that KBP with manual objective constraints resulted in better OAR sparing compared with KBP without manual objective constraints for single optimization, especially for the brainstem and spinal cord [24]. In the present study, we evaluated the DVH parameters for  $\ensuremath{\mathsf{KBP}}_{\ensuremath{\mathsf{ORIG}}}$  and then manually added the objective constraints for OARs to the optimization of the KBP<sub>CONST</sub>, whereas we did not change the objective constraints for PTV. Details of the objective constraints for KBPCONST are summarized in Table 3. Additionally, the priority of normal tissue objectives (NTO) was set to 200 for KBPCONST, although the default priority of 100 was used for  $KBP_{ORIG}$ . At our institution, the priority value of NTO was set at the same value as that of PTV, thus avoiding the creation of a high-dose region on the posterior side of the patient. For 14 patients with OPC and one with NPC, the KBPORG or KBPCONST were created using a single optimization without any planner intervention [2].

#### DVH analysis and plan quality evaluation

The DVH parameters of the KBPORIG, KBPCONST and CMO plans of the 15 patients of the validation set were compared in terms of the  $D_{98\%}$ ,  $D_{50\%}$  and  $D_{2\%}$  for the PTV, where  $D_{98\%}$ ,  $D_{50\%}$  and  $D_{2\%}$ are the doses received by 98, 50 and 2% of the PTV, respectively. In the present study, DVH parameters of the spinal cord, brainstem and parotid glands were evaluated, because these three OARs were the most important for IMRT plans: Dmax (maximum dose) of the spinal cord and brainstem, Dmed (median dose) and Dmean (mean dose) of the parotid glands. Moreover, the number of monitor units (MUs) and modulation complexity score for VMAT (MCSv) were evaluated 25, 26]. The ipsilateral and contralateral parotid glands were evaluated separately [3]. At our institution, treatment plans were created and evaluated according to the Japan Clinical Oncology Group (JCOG) 1015 protocol (Table 2) [27]. Paired t-tests were used to identify differences between KBPORIG, KBPCONST and CMO plans, with P-values < 0.01 considered to represent statistical significance.

Regarding plan quality, we evaluated the homogeneity index (HI; defined as [D<sub>2%</sub> - D<sub>98%</sub>]/D<sub>50%</sub>); the 95% isodose conformity index (CI<sub>95</sub>; defined as  $V_{95\%}/V_{PTV}$ ), where  $V_{95\%}$  is the volume covered by 95% of the prescribed dose and VPTV is the PTV volume; and DVH parameters of the KBP<sub>CONST</sub> and CMO plans [13, 28]. Additionally, the dose distributions of the KBP<sub>CONST</sub> and CMO plans of the 15 patients were compared by two expert radiation oncologists. The dose distributions of the KBP<sub>CONST</sub> were graded as superior, comparable or inferior to those of the CMO plan.

#### RESULTS

The DVH parameters for KBP<sub>ORIG</sub>, KBP<sub>CONST</sub> and CMO plans are summarized in Table 4. The mean PTV D98% and D2% for KBPORIG were 58.6 and 76.4 Gy, respectively. These values were significantly better than those of the KBP<sub>CONST</sub> (56.7 and 78.1 Gy; both P < 0.001) and CMO plans (54.6 and 79.3 Gy; both P < 0.01). The mean  $D_{2\%}$ of the PTV for KBP<sub>CONST</sub> was significantly smaller than that of the CMO plans (P < 0.0001), whereas the  $D_{98\%}$  and  $D_{50\%}$  of the PTV for  $KBP_{CONST}$  were comparable to those of the CMO plans.

In terms of OARs, the mean Dmax of spinal cord and brainstem for KBPORIG (72.1 and 65.8 Gy) were clinically unacceptable. The DVH parameters of KBP<sub>ORIG</sub> did not meet our goal for all OARs (Table 2). Thus, the KBPORIG was deemed unacceptable for clinical use. In contrast, for KBP<sub>CONST</sub>, the mean D<sub>max</sub> of spinal cord and the mean D<sub>med</sub> and D<sub>mean</sub> of contralateral parotid glands were comparable with those of the CMO plans; moreover, the mean D<sub>max</sub> of brainstem (48.8 Gy) and mean  $D_{\text{med}}$  and  $D_{\text{mean}}$  of ipsilateral parotid glands (26.2 and 31.9 Gy, respectively) for KBP  $_{\rm CONST}$  were significantly lower than those of the CMO plans. Thus, in terms of DVH parameters, KBPCONST were comparable with the CMO plans. The MU values of the KBP CONST and KBP OFFIC were significantly lower than those of the CMO plans (P < 0.001). MCSv of KBP<sub>CONST</sub> were larger than those of CMO plans, although the difference was not statistically significant

HI and CI95 of KBPCONST were also found to be comparable with those of the CMO plans. The dose distribution of the KBP CONST and CMO plans for the 15 patients were subsequently compared for all CT slices. Discussions between two expert radiation oncologists regarding

Table 3. Objective constraints for KBP<sub>CONST</sub>

8		Vol (%)	Dose (Gy)	Priority
PTV	Upper	0	70.7	175
	Upper	0	70.0	200
	Lower	100	69.3	200
	Lower	100	67.9	150
Brain	Upper	0	63.0	50
	Line	Automatically generated		
Brainstem	Upper	0	44.1	200
	Line	Automatically generated		
Left inner ear	Upper	0	56.0	50
	Line	Automatically generated		
Right inner ear	Upper	0	56.0	50
	Line	Automatically generated		
Larynx	Mean		31.5	Automatically generated
	Line	Automatically generated		
Mandible	Upper	50	42.0	50
	Line	Automatically generated		
Pharyngeal constrictor muscle	Upper	0	50.4	60
	Mean		35.0	60
	Line	Automatically generated		
Oral cavity	Upper	50	30.0	60
200/244/2424.454.	Line	Automatically generated		
Left parotid gland minus PTV	Upper	0	49.0	80
	Mean		18.0	100
	Line	Automatically generated		
Right parotid gland minus PTV	Upper	0	49.0	80
• •	Mean		18.0	100
	Line	Automatically generated		
Spinal cord	Upper	0	42.0	200
*	Upper	30	30.1	100
	Upper	50	24.5	100
	Line	Automatically generated		
Thyroid	Line	Automatically generated		
NTO				200

each of the 15 patients led to the conclusion that the KBP $_{\rm CONST}$  were superior to the CMO plans in seven cases (47%), comparable in six (40%) and inferior in two (13%).

Figure 1 shows the dose distributions in a patient with right tonsil cancer. In the KBP<sub>ORIG</sub> (Fig. 1A), the spinal cord was included in the high dose region; thus, the KBP<sub>ORIG</sub> was clinically unacceptable. In terms of the KBP<sub>CONST</sub> (Fig. 1B) and the CMO plan (Fig. 1C), there were no differences in PTV coverage and sparing of the spinal cord. In addition, the bilateral parotid glands were better spared by the KBP<sub>CONST</sub> than by the CMO plan. In this particular patient, the D<sub>med</sub> values of the ipsilateral and contralateral parotid glands for the CMO plan were 47.7 and 26.2 Gy, respectively. This patient's clinical plan could not fully meet our goal in terms of D<sub>med</sub> for parotid glands, although the planners accepted the plan finally after repeated re-optimization. In contrast, the D<sub>med</sub> of the ipsilateral and contralateral parotid glands for KBP<sub>CONST</sub> were 19.5 and 18.0 Gy, respectively. Thus, in this patient, the KBP<sub>CONST</sub> was superior in quality to the CMO plan.

#### DISCUSSION

The KBP<sub>ORIG</sub> and KBP<sub>CONST</sub> from a single optimization and CMO plans were compared. KBP<sub>ORIG</sub> was found to be clinically unacceptable due to high doses to important OARs including neurological structures. Similarly, Chang *et al.* showed that half of their KBP for patients with NPC did not achieve their DVH goals for neurologic structures [11]. Kamima *et al.* reported that KBP could not achieve their study criteria for the spinal cord and brainstem without manual objective constraints from a single optimization [24]. On the other hand, in the present study, KBP<sub>CONST</sub> from a single optimization was comparable or superior to CMO plans for most patients with head and neck cancer. The difference between KBP<sub>ORIG</sub> and KBP<sub>CONST</sub> was manual setting of objective constraints for OARs. Our study revealed the importance of adding objective constraints for KBP from a single optimization.

Hussein et al. demonstrated that KBP from a single optimization and using automatically generated objective constraints were acceptable in the pelvic region [13], because there are fewer OARs in the

Table 4. DVH parameters for PTV and OARs, and MU and MCSv for KBPCONST, KBPORIG and CMO plans

	Parameter	(a) KBP <sub>CONST</sub> (Gy)	(b) KBP <sub>ORIG</sub> (Gy)	(c) CMO plans (Gy)	P-value
PTV	$D_{98\%}$	$56.7 \pm 2.5$	$58.6 \pm 2.2$	$54.6 \pm 3.9$	a vs b: 0.0003
					b vs c: 0.004
	D <sub>50%</sub>	$72.9 \pm 0.4$	$71.5 \pm 1.8$	$73.0 \pm 0.4$	NS
	$D_{2\%}$	$78.1 \pm 1.0$	$76.4 \pm 0.9$	$79.3 \pm 1.5$	a vs b: 0.0005
					b vs c: <0.0001
					a vs c: <0.0001
Spinal cord	$D_{max}$	$47.7 \pm 1.1$	$72.1 \pm 4.1$	$47.3 \pm 2.3$	a vs b; < 0.0001
					b vs c: <0.0001
Brainstem	$D_{max}$	$48.8 \pm 1.5$	$65.8 \pm 2.0$	$52.9 \pm 4.4$	a vs b: <0.0001
					b vs c: <0.0001
					a vs c: 0.0006
Ipsilateral parotid gland	$D_{med}$	$26.2\pm11.1$	$44.4 \pm 8.5$	$36.1 \pm 13.4$	a vs b: <0.0001
, , ,					b vs c: 0.003
					a vs c: 0.002
	$\mathbf{D}_{\text{mean}}$	$31.9 \pm 7.8$	$45.5 \pm 6.1$	$38.7 \pm 10.2$	a vs b: <0.0001
					b vs c; 0.002
					a vs c: 0.006
Contralateral parotid gland	$\mathbf{D}_{\mathrm{med}}$	$22.5 \pm 3.9$	$40.2 \pm 7.0$	$22.2 \pm 8.2$	a vs b: <0.0001
1.57					b vs c: <0.0001
	$D_{mean}$	$28.7 \pm 4.4$	$42.6 \pm 5.5$	$28.0 \pm 6.6$	a vs b: <0.0001
					b vs c: <0.0001
MU		$490 \pm 31$	$448 \pm 28$	$561 \pm 68$	b vs c: 0.0001
					a vs c: 0.0001
MCSv		$\boldsymbol{0.29 \pm 0.02}$	$0.32 \pm 0.02$	$0.28 \pm 0.03$	a vs b: 0.0003
					b vs c: 0.0002

pelvic region than in the head and neck region. The anatomical complexity of the head and neck region hinders the achievement of DVH goals for pharyngeal cancer. Most investigators have used only automatically generated objective constraints for OARs when comparing DVH parameters between KBP and CMO plans [2, 4, 6, 7, 11, 13-15, 22, 23]. However, in the present study, the KBP from a single optimization with manual addition of objective constraints to PTV and OARs were comparable to or better than CMO plans in 87% of patients. These adopted objective constraints for OARs were found by trial and error to improve the worst CMO plan of the 55 patients in the training set. In addition, we set objective constraints to meet our goals, especially for  $neurological \, structures, by \, setting \, priority \, of \, spinal \, cord \, and \, brainstem$ strictly (Table 3). Only line objectives were used for constraints of OARs in KBP<sub>ORIG</sub>. Similarly, the previous studies described that line objectives were weak for important structures such as the spinal cord and brainstem [11, 24]. Thus, setting objective constraints manually was an important factor for the clinical application of KBP.

In two of the 15 patients, the dose distribution of the KBP $_{\rm CONST}$  was clinically inferior to that of the CMO plans, although the DVH parameters of the PTV and OARs, HI and CI $_{95}$  were comparable. As hot spots in the larynx were noted in the both cases, the plans were regarded as inferior to the CMO plans. Many investigators do not evaluate dose distributions clinically [2–4, 11, 13, 23]. Both comprehensive

assessment of each plan by radiation oncologists and evaluation of DVH parameters were necessary for evaluation of KBP.

In this study, KBP<sub>CONST</sub> and KBP<sub>ORIG</sub> resulted in a significant reduction in the number of MUs compared with CMO plans (P < 0.001). Kubo et al. stated that increased MUs in KBP for prostate cancer implied that KBP are more complicated to deliver than CMO plans [2]. However, the results of this study including MCSv suggest that KBP might reduce plan complexity when appropriate objective constraints were used.

Finally, KBP<sub>CONST</sub> could resolve the limitation of the time-consuming optimization process. Approximately 1-2 h were required to create each of the CMO plans with repeated re-optimization, whereas a single optimization of each KBP<sub>CONST</sub> took only 15 min. In addition, KBP<sub>CONST</sub> from a single optimization also reduced the dependence on the planners' ability, meaning that less-experienced planners could produce good-quality plans [11, 29].

In conclusion, KBP $_{\rm ORIG}$  was found to be clinically unacceptable, while KBP $_{\rm CONST}$  from a single optimization was comparable with or superior to CMO plans for most patients with head and neck cancer. Manual addition of appropriate objective constraints improved both KBP plan quality and DVH parameters. KBP $_{\rm CONST}$  can overcome the limitation of the consuming lengthy optimization process and shows good potential for clinical use.

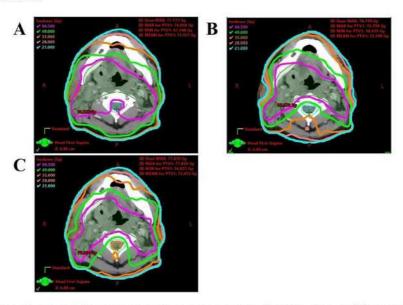


Fig. 1. (A) KBP without manual objective constraints from a single optimization for right tonsil cancer, (B) KBP with manual objective constraints from a single optimization for the same patient, and (C) CMO plan for the same patient. Green line, 49 Gy iso-dose line; orange line, 35 Gy iso-dose line.

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#### CONFLICT OF INTEREST

None.

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#### REFERENCES

- Nishi T, Nishimura Y, Shibata T et al. Volume and dosimetric changes and initial clinical experience of a two-step adaptive intensity modulated radiation therapy (IMRT) scheme for head and neck cancer. Radiother Oncol. 2013;106:85–9.
- Kubo K, Monzen H, Ishii K et al. Dosimetric comparison of RapidPlan and manually optimized plans in volumetric modulated arc therapy for prostate cancer. *Phys Med.* 2017;44: 199–204.

- Fogliata A, Reggiori G, Stravato A et al. RapidPlan head and neck model: The objectives and possible clinical benefit. Radiat Oncol. 2017;12:73.
- Hazell I, Bzdusek K, Kumar P et al. Automatic planning of head and neck treatment plans. J Appl Clin Med Phys. 2016;17:272–82.
- Tamura M, Monzen H, Matsumoto K et al. Mechanical performance of a commercial knowledge-based VMAT planning for prostate cancer. Radiat Oncol. 2018;13:163.
- Ueda Y, Fukunaga JI, Kamima T et al. Evaluation of multiple institutions' models for knowledge-based planning of volumetric modulated arc therapy (VMAT) for prostate cancer. Radiat Oncol. 2018;13:46. doi: 10.1186/s13014-018-0994-1.
- Tol JP, Delaney AR, Dahele M et al. Evaluation of a knowledgebased planning solution for head and neck cancer. Int J Radiat Oncol Biol Phys. 2014;91:612–20.
- Wang J, Chen Z, Li W et al. A new strategy for volumetricmodulated arc therapy planning using AutoPlanning based multicriteria optimization for nasopharyngeal carcinoma. *Radiat Oncol.* 2018;13:94. doi: 10.1186/s13014-018-1042-x.
- Tol JP, Dahele M, Delaney AR et al. Can knowledge-based DVH predictions be used for automated, individualized quality assurance of radiotherapy treatment plans? *Radiat Oncol.* 2015;10: 234
- Delaney AR, Tol JP, Dahele M et al. Effect of dosimetric outliers on the performance of a commercial knowledge-based planning solution. Int J Radiat Oncol Biol Phys. 2015;94: 469-77.

- 11. Chang ATY, Hung AWM, Cheung FWK et al. Comparison of planning quality and efficiency between conventional and knowledge-based algorithms in nasopharyngeal cancer patients using intensity modulated radiation therapy. Int J Radiat Oncol Biol Phys. 2016:95:981-90.
- 12. Hussein M. Heijmen BIM, Verellen D et al. Automation in intensity modulated radiotherapy treatment planning-A review of recent innovations. Br J Radiol. 2018;91:20180270.
- 13. Hussein M, South CP, Barry MA et al. Clinical validation and benchmarking of knowledge-based IMRT and VMAT treatment planning in pelvic anatomy. Radiother Oncol. 2016;120:473-9.
- 14. Fogliata A, Belosi F, Clivio A et al. On the pre-clinical validation of a commercial model-based optimisation engine: Application to volumetric modulated arc therapy for patients with lung or prostate cancer, Radiother Oncol, 2014:113:385-91.
- 15. Krayenbuehl J, Norton I, Studer G et al. Evaluation of an automated knowledge based treatment planning system for head and neck. Radiat Oncol. 2015;10:226.
- 16. Lu L, Sheng Y, Donaghue J et al. Three IMRT advanced planning tools: A multi-institutional side-by-side comparison. J Appl Clin Med Phys. 2019;20:65-77.
- 17. Nishimura Y, Shibata T, Nakamatsu K et al. A two-step intensitymodulated radiation therapy method for nasopharyngeal cancer: The Kinki university experience. Jpn J Clin Oncol. 2010;40: 130 - 8.
- 18. Tatebe H, Doi H, Ishikawa K et al. Two-step intensity-modulated radiation therapy for oropharyngeal cancer initial clinical experience and validation of clinical staging. Anticancer Res. 2018; 38:979-86.
- 19. Grégoire V, Levendag P, Ang KK et al. CT-based delineation of lymph node levels and related CTVs in the node-negative neck: DAHANCA, EORTC, GORTEC, NCIC, RTOG consensus guidelines. Radiother Oncol. 2003;69:227-36.
- 20. Eisbruch A. Foote RL, O'Sullivan B et al. Intensity-modulated radiation therapy for head and neck cancer: Emphasis on the

- selection and delineation of the targets. Semin Radiat Oncol. 2002:12:238-49.
- Suzuki M, Nishimura Y, Nakamatsu K et al. Analysis of interfractional set-up errors and intrafractional organ motions during IMRT for head and neck tumors to define an appropriate planning target volume (PTV)- and planning organs at risk volume (PRV)margins. Radiother Oncol. 2006;78:283-90.
- Fogliata A, Nicolini G, Clivio A et al. A broad scope knowledge based model for optimization of VMAT in esophageal cancer: Validation and assessment of plan quality among different treatment centers. Radiat Oncol. 2015;10:220.
- 23. Wang M, Li S, Huang Y et al. An interactive plan and model evolution method for knowledge-based pelvic VMAT planning. J Appl Clin Med Phys. 2018;19:491-8.
- 24. Kamima T, Ueda Y, Fukunaga J et al. Multi-institutional evaluation of knowledge-based planning performance of volumetric modulated arc therapy (VMAT) for head and neck cancer. Phys Med. 2019;64:174-81.
- 25. Masi L, Doro R, Favuzza V et al. Impact of plan parameters on the dosimetric accuracy of volumetric modulated arc therapy. Med Phys. 2013;40:071718.
- 26. McNiven A, Purdie T. A new metric for assessing IMRT modulation complexity and plan deliverability. Med Phys. 2010;37:505-15.
- 27. Nishimura Y, Kodaira T, Itou Y et al. A phase II study of intensity modulated radiation therapy (IMRT) with chemotherapy for locoregionally advanced nasopharyngeal cancer (NPC) (JCOG1015): Acute toxicity and treatment compliance. Int J Radiat Oncol Biol Phys 2016;96:E334.
- Kataria T, Sharma K, Subramani V et al. Homogeneity index: An objective tool for assessment of conformal radiation treatments. J Med Phys. 2012;37:207-13.
- Kubo K, Monzen H, Ishii K et al. Inter-planner variation in treatment-plan quality of plans created with a knowledge-based  $treatment\ planning\ system.\ Phys\ Med.\ 2019; 67: 132-40.$